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of

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for

SCREENING METHOD AND APPARATUS



Use of known conventional metal detectors, whether portals or wands, would not be efficient for this purpose. Conventional systems generate an audio-band oscillating or pulsed magnetic field with which they illuminate the subject. The time-varying field induces electrical eddy currents in metallic objects. It is these eddy currents which are detected by the system, to reveal the presence of the metallic objects.

## BRIEF SUMMARY OF THE INVENTION

The present invention provides an apparatus and a method for scanning a subject for the presence of an object which is either permanently magnetic or susceptible to being magnetized by an external field. The sensors in this scanning apparatus can be mounted on a portal type frame. This positions the entire sensor array in proximity to a subject. The portal arrangement of the scanner arranges the sensors suitably for positioning every sensor in proximity to the body of a subject, as the subject passes through the portal.

The sensors can detect the magnetic field of the object, whether the object is a permanent magnet or merely susceptible to magnetization. Where an external field induces a magnetic field in the object, the external field may be the Earth's magnetic field, or it may be generated by another source, such as a nearby MRI apparatus or a dedicated source such as one mounted on the frame of the apparatus.

The novel features of this invention, as well as the invention itself, will be best understood from the attached drawings, taken along with the following description, in which similar reference characters refer to similar parts, and in which:

## BRIEF DESCRIPTION OF THE SEVERAL VIEWS OF THE DRAWINGS

Figure 1 is a schematic showing the horizontal arrangement of sensor arrays in a first portal type embodiment;

Figure 2 is a schematic of a second portal embodiment;

Figure 3 is a schematic of a third portal embodiment;

Figure 4 is a schematic of the arrangement of a permanent magnet source relative to the sensing axis of the sensor;

Figure 5 is a schematic showing the arrangement of the source field from a permanent magnet, a sensor, and a ferromagnetic object;

Figure 6 is a schematic showing the magnetic field of the ferromagnetic object shown in Figure 5;

5        Figure 7 is a schematic showing the arrangement of a sensor and the source field from two permanent magnets;

Figures 8 and 9 show a first embodiment of the excitation coil configuration relative to the portal structure;

Figures 10 and 11 show a second embodiment of the excitation coil configuration  
10        relative to the portal structure; and

Figures 12 and 13 show a third embodiment of the excitation coil configuration relative to the portal structure.

#### DETAILED DESCRIPTION OF THE INVENTION

15        The present invention, which applies to both permanently magnetic objects called “hard” ferromagnets and non-permanent magnetically susceptible objects called “soft” ferromagnets, can use magnetometers with good sensitivity at frequencies all the way, or nearly, to DC, i.e., zero frequency. This allows several modes of use:

(1) As a completely passive system, the present invention detects ferromagnetic  
20        objects using their permanent magnetization, in the case of “hard” ferromagnets, or the magnetization induced by the Earth’s magnetic field, in the case of “soft” ferromagnets.

(2) As a DC magnetic susceptometer, the present invention applies a static DC magnetic field, allowing control and usually enhancement of the magnetization of soft ferromagnets, thus enhancing their detectability.

25        (3) As an AC magnetic susceptometer, the present invention applies an oscillating AC magnetic field, but at very low frequencies compared to conventional detectors, allowing enhancement of their magnetization. The purpose of AC illumination is to move the signal from DC to a region of lower noise at finite frequency. The AC frequency is preferably chosen to avoid inducing the electrical eddy currents detected by

other systems, to suppress the response from non-ferromagnetic metal objects, and thus maintaining the discrimination capability.

The present invention importantly arranges an array of sensors in such a way that the entire sensor array can be placed in proximity to the body of a subject, such as a patient or an attendant. Further, the sensor arrays can be arranged so as to be susceptible to placement in proximity to the body of a subject, such as a patient lying recumbent, as on a stretcher or gurney.

A passive magnetic embodiment of the portal used in one embodiment of the present invention can be similar in some respects to the SecureScan 2000<sup>TM</sup> weapons detection portal which is manufactured by Quantum Magnetics, Inc., and marketed by Milestone Technology, Inc., or the *i-Portal*<sup>TM</sup> weapons detection portal which is marketed by Quantum Magnetics, Inc.

The portal includes two panels of sensors on the sides of the entryway. An array of magnetometers inside each panel enables detection, characterization, and localization of ferromagnetic objects from the soles of the feet to the top of the head. The magnetometer array can take a variety of configurations, and it can use a variety of sensor technologies. For example, a set of 16 single-axis magnetic gradiometers can be arranged with 8 in each panel. Other configurations can include arrays of multi-axis gradiometers, or combinations of single-axis and multi-axis gradiometers. One or more magnetic tensor gradiometers may also be used. A magnetoresistive magnetometer, or any other sensor capable of sensing magnetic field changes at or near zero frequency, can be used.

As shown in Figure 1, in order to scan a patient on a gurney, the portal sensor configuration 10 of the present invention can be arranged to bring all of the sensors closer to the patient and to effectively scan a patient in the recumbent position. Rather than being arranged vertically, the two sensor panels 12, 14 can be arranged horizontally, parallel to the path of the gurney and on either side, as shown in Figure 1. This places the sensors in a similar relation to the patient as they would have, in the vertical arrangement, to an ambulatory patient. Also, a single “snapshot” of data covers the

entire gurney and patient, as in the ambulatory case. The sensor panels 12, 14 can be permanently arranged horizontally, or they can pivot to this configuration.

Alternatively, in addition to the vertically arranged sensor panels as in the aforementioned known portals, the portal can have a “dutch door” with an additional,  
5 horizontal, sensor panel 16 in the upper half of the door, just high enough to clear a patient on a gurney, as shown in Figure 2. As the patient is wheeled under the upper door, the patient would pass in close proximity to the horizontal sensor panel 16, allowing all of its sensors to scan the patient from head to foot, or vice versa. This gives the best detection and resolution of objects, since more sensors are placed closer to the  
10 patient. Then, the attendant would push the dutch door open and walk through the portal, being scanned by the vertically arranged sensor panels. The “dutch door” array 16 can be spring loaded, so that it moves out of the way for an ambulatory subject. A microswitch indicator can tell the software whether the door is engaged, for a recumbent patient, or disengaged, for an ambulatory subject. As a variation of this embodiment, a portal with  
15 vertically arranged sensor panels can be situated next to a portal with a horizontally arranged sensor panel, as shown in Figure 3.

As an alternative to the passive magnetic portal, an AC or DC magnetizing field can be provided by one or more source coils, a DC field can be provided by a permanent magnet array, or a DC field can be provided in the form of the fringing field of a nearby  
20 MRI magnet. In any case, a computer is provided to interrogate the sensors and to interpret the magnetic signals, to detect, characterize, and locate ferromagnetic objects. Characterization of the object provides the size and orientation of its magnetic moment, which can be related to the physical size of the object, and to the magnitude of the attractive magnetic force. The analysis software can use various known algorithms, or a  
25 neural network can be used. The information gained can be related to a photographic image of the subject, for the purpose of locating the ferromagnetic object on the subject. A light display can be used to indicate the approximate location of the detected object. System diagnosis, monitoring, and signal interpretation can be done via the Internet, if desired.

The use of AC fields enables the use of induction coil sensors, in addition to or instead of magnetometers, like magnetoresistive, fluxgate, and other types. Induction coil sensors are impossible to use in the DC embodiment because the induction coil has zero sensitivity at zero frequency. Using induction coil sensors typically reduces the cost of the product without sacrificing sensitivity in the AC system.

An AC system could make use of two different excitation directions – operating at two different frequencies, to avoid crosstalk – which can improve detection of long, narrow objects, which are precisely the shape that is most dangerous in this situation.

The excitation frequency is chosen to be low enough so that the magnetization (or, equivalently, magnetic susceptibility) response of objects to be detected exceeds their eddy current response. The choice of frequency is expected to be less than 1 kHz, but it can be as high as 3 kHz in some applications.

The excitation current can be driven by any number of standard drive circuits, including either direct drive (controlled voltage source in series with the coil) or a resonant drive (voltage source coupled to the coil via a series capacitance whose value is chosen such that, in combination with the coil's self-inductance, the current is a maximum at a desired resonant frequency given by  $1/2\pi(LC)^{1/2}$ ).

The receiver or sensor coil can be made of two coils, wound in opposite senses and connected in series. They form what is well-known as a gradiometer; a uniform magnetic flux threading both coils produces zero response. The coils are distributed symmetrically relative to the excitation coil such that, in the absence of any target object (which is conductive, magnetic or magnetically permeable) nearby, each senses an identical flux from the excitation which thus cancels out.

Although the intent is to make the two coils perfectly identical, and to place them in identically symmetric locations, in practice one falls short of the ideal. As a result, any actual embodiment will display a nonzero response to the excitation, even in the absence of a target; this residual common-mode signal is referred to as an “imbalance” signal. Standard electrical circuits can zero out the imbalance signal by adding an appropriately scaled fraction of the reference voltage  $V_{\text{ref}}$  (a voltage proportional to the excitation current, obtained by measuring across a series monitor resistor) to the output voltage  $V_{\text{out}}$ .

When a target object is near to either coil, it spoils the symmetry and thus induces a finite signal. This signal oscillates at the same frequency as the excitation. Standard demodulation or phase-sensitive detection circuits, using  $V_{\text{ref}}$  as the phase reference, measure the magnitude of  $V_{\text{out}}$  in phase with  $V_{\text{ref}}$  and in quadrature (90 degrees out of phase) with  $V_{\text{ref}}$ . At an appropriately chosen low frequency, the response will be dominated by the susceptibility response, which appears predominantly in the quadrature output, as opposed to the eddy current response, which appears predominantly in the in-phase component.

In principle, the coils could be replaced by two magnetometer sensors (fluxgate, magnetoresistive, magnetoimpedance, etc.). Coils respond to the time derivative of the magnetic field, while magnetometers respond to the field itself; the coil's output voltage is shifted by 90 degrees with respect to a magnetometer's. If magnetometers are used instead of coils, then the susceptibility response would show up in the in-phase component and the eddy current response (at low frequency) in the quadrature component.

If the operating frequency is chosen much too high, both susceptibility and eddy-current responses appear in the in-phase component (using magnetometers) or quadrature component (using coils), but with opposite sign, making it impossible to distinguish between the two. At intermediate frequencies, the eddy current phase is intermediate between the two components, complicating the distinction. Therefore, it is important to choose the excitation frequency to be low enough, and preferably less than about 3000 Hz.

The substrate or coil form must be nonconductive, nonferromagnetic and, with one possible exception, magnetically impermeable ( $\mu = \mu_0$ , where  $\mu_0$  is the permeability of free space). The exception is that a magnetically permeable core inside sensor coils having a cylindrical geometry can increase the sensitivity of the system.

The use of a reference sensor helps to eliminate common mode error signals. For instance, a nearby passenger conveyer, such as a gurney, could contain magnetic components, but this spurious magnetization is not what is intended to detect, and, therefore, it is preferable to eliminate this magnetic source.

An audio alert, such as a buzzer, and/or an alarm light can be employed to signal the presence of an unwanted ferromagnetic object.

As shown in Figure 4, the sensor's sensitivity axis is orthogonal to the axis of the magnetic field of a permanent magnet 32. Otherwise stated, the magnetic field of the permanent magnet 32 is normal to the plane of the sensor 34.

In Figure 5, the magnetic field of the DC permanent magnet field source 32 magnetizes the ferromagnetic object, which then has a magnetic field of its own, as shown in Figure 6. This induced magnetization ("demag field") is detected by the sensor 34, triggering the alarm buzzer and/or light.

An alternative configuration, shown in Figure 7, utilizes two permanent magnets 32A, 32B, as the magnetic field between them is less divergent than with a single permanent magnet. With the use of two permanent magnets 32A, 32B and less resultant divergence, there is less need for criticality about positioning the permanent magnet with respect to the sensor 34.

Figures 8 through 13 show various embodiments of the excitation coil configurations useful with the portal structure, for applying a magnetizing field to the volume of space around a portal, in accordance with the present invention. For the sake of illustration, the portal is assumed to comprise a set of single-axis magnetic field gradiometers in two substantially equal arrays on either side of the opening. The principles can be generalized to portals with gradiometers in other orientations, and with multi-axis gradiometers as well.

The underlying requirement of the applied field is that it should not disturb the sensors. That is, in the absence of a magnetic or magnetizable object in the portal, the field should produce zero signal on the gradiometer outputs. This requirement ensures that variations in the applied field don't show up as noise on the sensors – since the objective is to increase the signal from objects, by increasing the magnetizing field, without increasing the sensor noise.

The requirement can be stated as follows: the magnetizing field should have zero mutual inductance with the sensors. This can be expressed in two forms, with the same net result but with slightly different implementation issues. In one form, the magnetizing

field has zero mutual inductance with each magnetometer (a pair of them making one gradiometer). This is a more restrictive requirement than the second form, which specifies zero mutual inductance with each gradiometer.

Assume a coordinate system in which the z-axis points vertically, the x-axis horizontally in the plane of the portal, and the y-axis orthogonally to the plane of the portal. Figures 8 through 13 all assume gradiometers measuring the difference in the x-direction of the x-component of the field (written as  $\partial B_x/\partial x$ ). Figures 8 through 11 illustrate the first form of the requirement (zero coupling to each magnetometer); this is achieved by making the field point entirely in the y-direction (orthogonally to the sensitive axis) at all the sensors.

Figures 8 and 9 illustrate a single coil in the portal plane, with Figure 8 showing the front elevation of the portal, and Figure 9 showing the right side elevation. Not only is the illustrated coil 40 in the plane of the portal, or as close as possible to it, but the vertical legs run midway between each pair of magnetometers 42A, 42B making up the gradiometer pair 42. Thus, not only is the field perpendicular to the magnetometers' sensitive axis, but each sensor of the pair sees the same field, so any residual field gets canceled on subtraction of one sensor signal from the other, to form the gradient measurement. The coil 40 need not be higher or lower than the portal panels 43A, 43B; the components are just shown this way for clarity.

Figures 10 and 11 show a pair of coils 44, 46 on either side of the portal plane, with Figure 10 showing the front elevation of the portal, and Figure 11 showing the right side elevation. This optimum arrangement is as a Helmholtz coil pair, but this is not mandatory. The Helmholtz configuration gives the best field uniformity over the portal aperture, but it can add some bulkiness to the apparatus, which can create a problem in some applications, such as an especially "space-challenged" MRI facility. The two coils 44, 46 overlap. Current runs in the same direction, clockwise in Figure 10, in both coils.

Figures 12 and 13 illustrate the second form of the requirement (zero mutual inductance with each gradiometer). In this embodiment, each of two coils 48, 50 creates a field in the x-direction. Figure 12 shows the front elevation of the portal, and Figure 13 shows the right side elevation. Positioning is chosen to make the magnetizing field the

same at both magnetometers 42A, 42B in each gradiometer 42. Each magnetometer 42A, 42B is located at one end of one of the thin lines denoting the gradiometers 42. By making the excitation field substantially identical for each magnetometer 42A, 42B, the differential (gradient) measurement substantially cancels out the excitation field. The  
5 two coils 48, 50 overlap in the view shown in Figure 13, and they carry current in the same direction, clockwise in the drawing.

While the particular invention as herein shown and disclosed in detail is fully capable of obtaining the objects and providing the advantages hereinbefore stated, it is to be understood that this disclosure is merely illustrative of the presently preferred  
10 embodiments of the invention and that no limitations are intended other than as described in the appended claims.